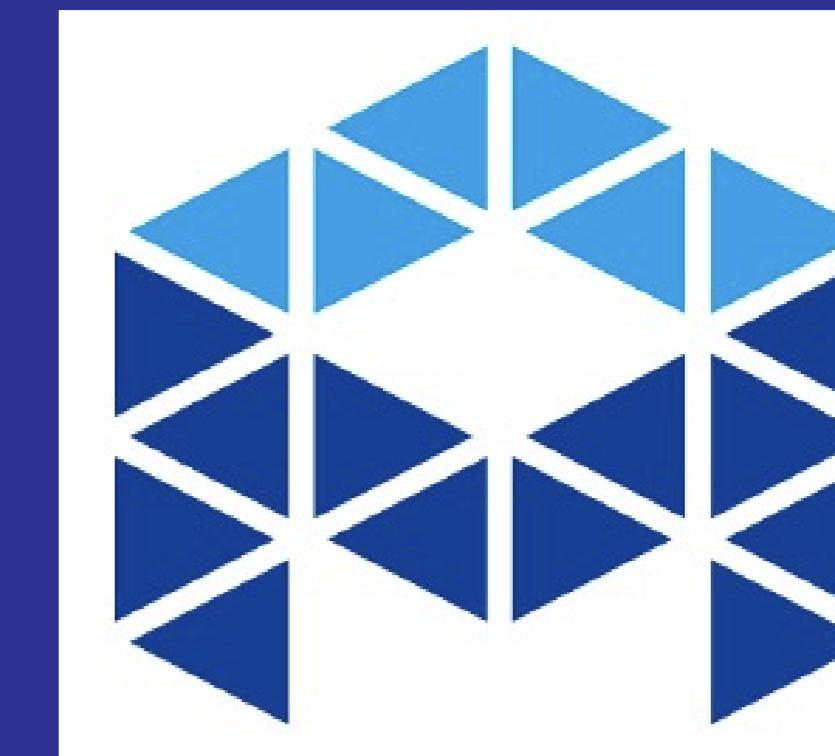
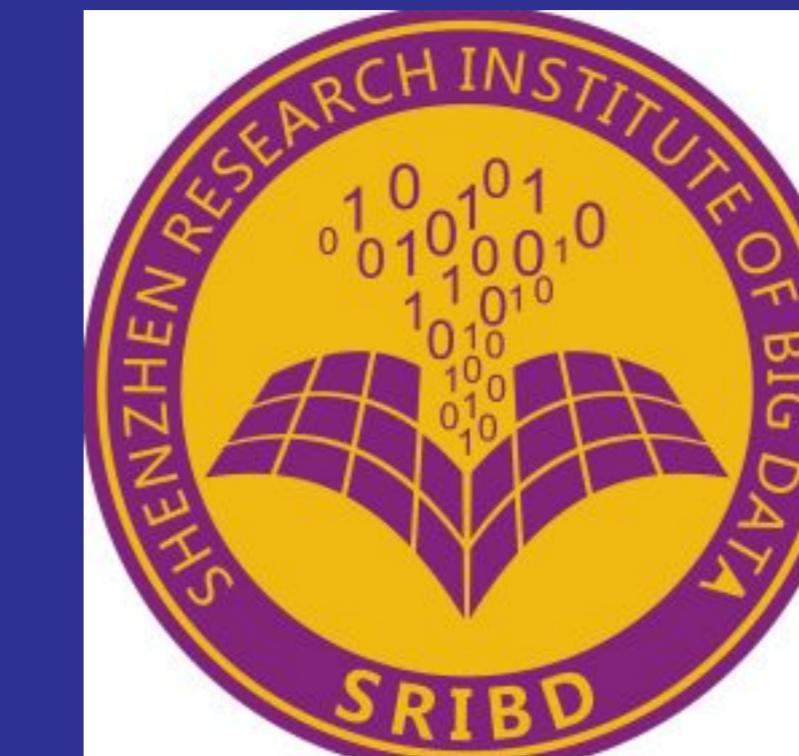


Iterative Convolution-Thresholding method for interface related optimization problems

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Introduction & Background

Interface related optimization problems arise from many applications including image segmentation; heat sink design; structure, shape and topology optimization; optimal composite material; fluid network design; and so on.

► The Mathematical Problem

$$\begin{aligned} \min_{\Omega_0} \mathcal{J}(\Omega_0, \Theta) \\ \text{s.t. } C(\Omega_0, \Theta) = 0. \end{aligned}$$

where

► $\mathcal{J}(\Omega_0, \Theta)$: objective functional

► $\Omega_0 \subset \Omega$: domain to be optimized in a computational domain Ω

► Θ : possible state variables (e.g. velocity field, temperature, etc.)

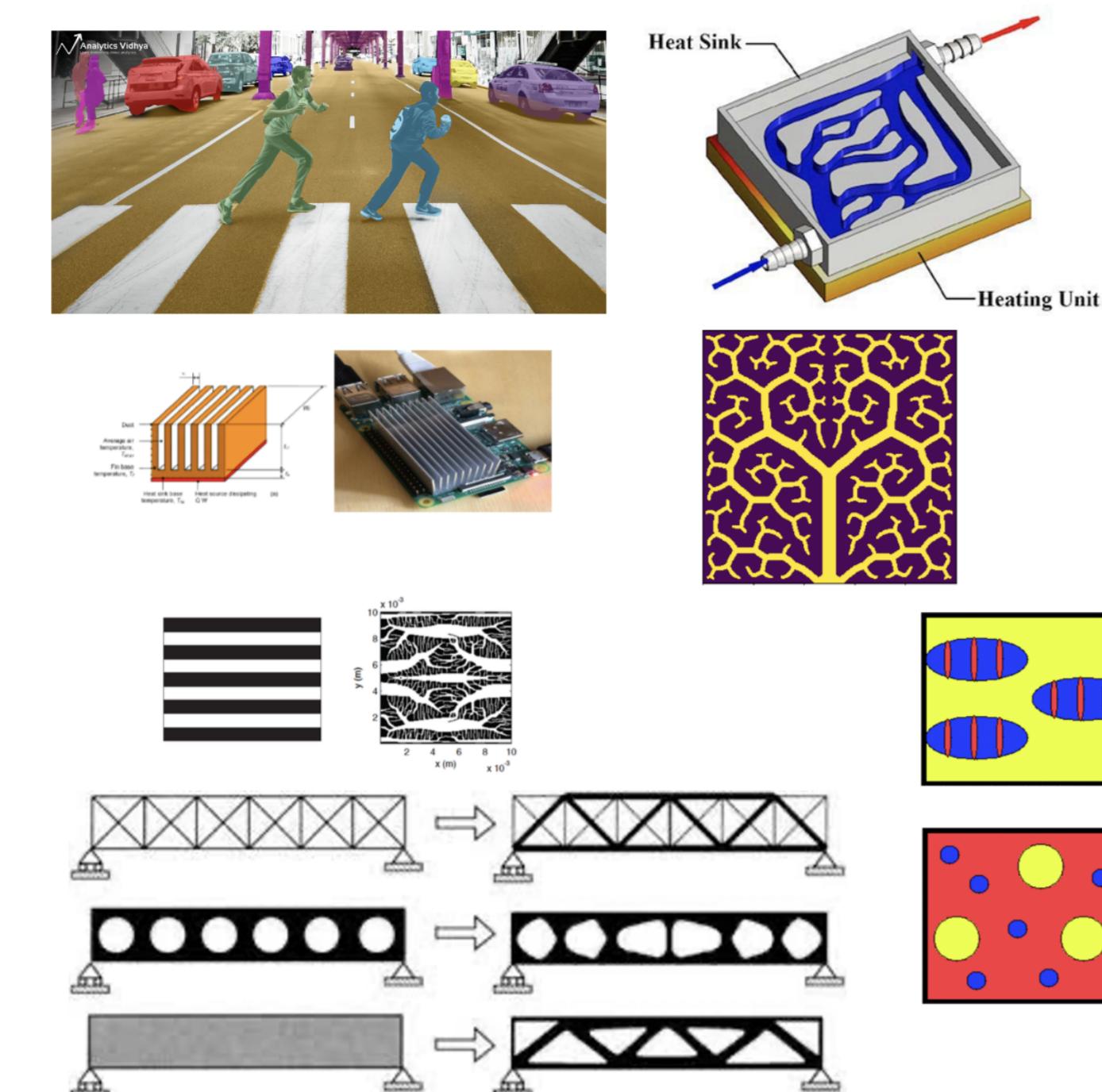


Figure 1: Interface related optimization problems

Mathematical modelling and simulation of the problem:

Representation of the interface
Approximation of the problem
Numerical methods

We propose a framework algorithm based on the indicator function representation.

The mathematical problem

► The general formula:

$$(u^*, \Theta^*) = \arg \min_{u \in \mathcal{B}, \Theta \in \mathcal{S}} \mathcal{E} := \sum_{i=1}^n \int_{\Omega_i} F_i(\Theta_1, \dots, \Theta_n) dx + \lambda \sum_{i=1}^n |\partial \Omega_i|.$$

$$\mathcal{B} = \left\{ (u_1, u_2, \dots, u_n) \in BV(\Omega, \mathbb{R}^n) \mid u_i = \{0, 1\} \text{ and } \sum_{i=1}^n u_i(x) = 1 \right\},$$

► \mathcal{S} : admissible set of $\Theta = (\Theta_1, \Theta_2, \dots, \Theta_n)$.

► The indicator function representation:

$$u_i(x) = \chi_{\Omega_i}(x) := \begin{cases} 1 & \text{if } x \in \Omega_i, \\ 0 & \text{otherwise,} \end{cases} \quad i \in [n].$$

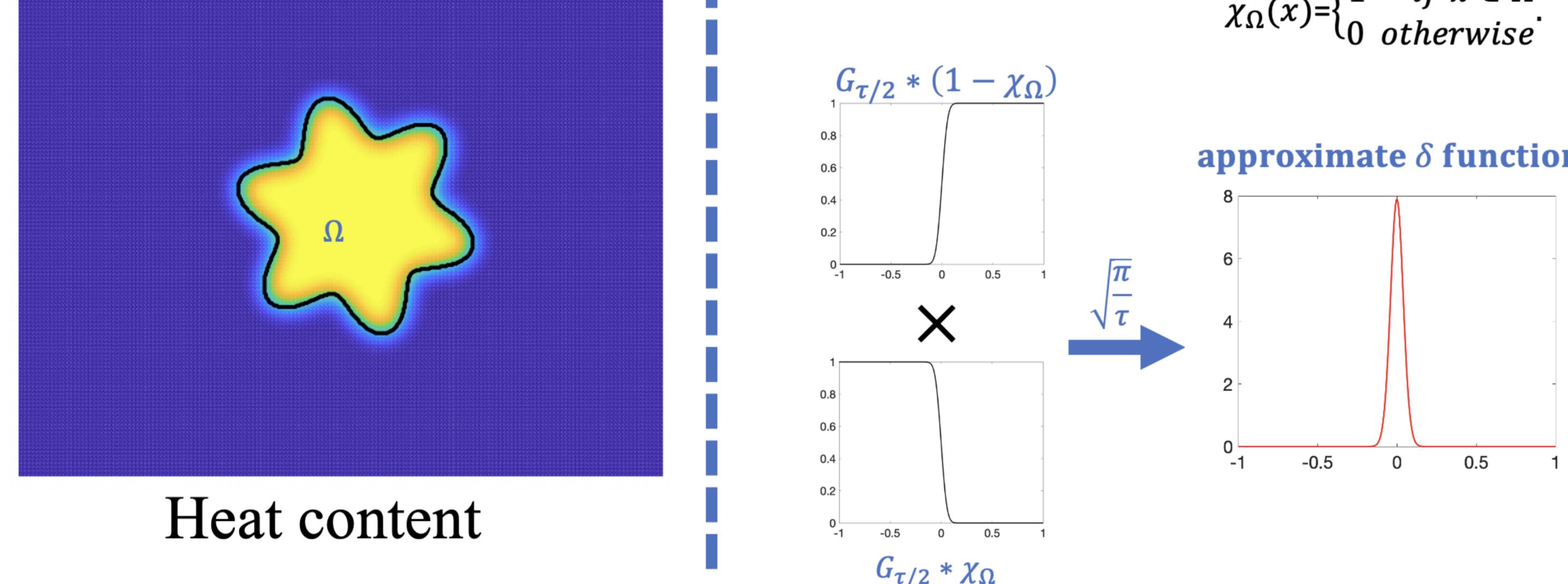
► The approximation: When $\tau \ll 1$, the length of $\partial \Omega_i \cap \partial \Omega_j$ can be approximated by [Eshedoglu + Otto, CPAM, 2015]

$$|\partial \Omega_i \cap \partial \Omega_j| \approx \sqrt{\frac{\pi}{\tau}} \int_{\Omega} u_i G_{\tau} * u_j dx,$$

where $*$ represents convolution and

$$G_{\delta t}(x) = \frac{1}{(4\pi\tau)^{d/2}} \exp\left(-\frac{|x|^2}{4\tau}\right)$$

is the heat kernel for the d -dimensional heat diffusion equation in free space.



► The approximate problem:

$$\mathcal{E}^{\tau}(u, \Theta) = \sum_{i=1}^n \left[\int_{\Omega} u_i F_i(\Theta_1, \dots, \Theta_n) dx + \lambda \sum_{j=1, j \neq i}^n \sqrt{\frac{\pi}{\tau}} \int_{\Omega} u_i G_{\tau} * u_j dx \right].$$

Derivation of the method

Apply the coordinate descent method to minimize $\mathcal{E}^{\tau}(u, \Theta)$; that is, starting from an initial guess: u^0 , we find the minimizers iteratively in the following order:

$$\Theta^0, u^0, \Theta^1, \dots, u^k, \Theta^k, \dots$$

where

$$\Theta^k = \min_{\Theta \in \mathcal{S}} \sum_{i=1}^n \int_{\Omega} u_i^k F_i(\Theta_1, \dots, \Theta_n) dx \quad (1)$$

$$u^{k+1} = \min_{u \in \mathcal{B}} \sum_{i=1}^n \int_{\Omega} u_i F_i(\Theta_1^k, \dots, \Theta_n^k) dx + \lambda \sum_{j=1, j \neq i}^n \sqrt{\frac{\pi}{\tau}} \int_{\Omega} u_i G_{\tau} * u_j dx \quad (2)$$

Since $\mathcal{E}^{\tau}(u, \Theta)$ is concave in u , solution to (2) can be approximated by solving the relaxed and linearized problem.

$$u^{k+1} = \arg \min_{u \in \mathcal{K}} \mathcal{L}^{\tau}(f, \Theta^k, u^k, u)$$

Derivation of the method

$$\mathcal{L}^{\tau}(f, \Theta^k, u^k, u) = \sum_{i=1}^n \int_{\Omega} u_i \phi_i^k dx$$

$$\phi_i^k = F_i(\Theta_1^k, \dots, \Theta_n^k) + \lambda \sum_{j=1, j \neq i}^n \sqrt{\frac{\pi}{\tau}} G_{\tau} * u_j^k$$

$$\mathcal{K} = \{(u_1, u_2, \dots, u_n) \in BV(\Omega, \mathbb{R}^n) \mid u_i \in [0, 1], \text{ and } \sum_{i=1}^n u_i(x) = 1\}$$

The Iterative Convolution-Thresholding Method (ICTM)

1. For the fixed u^s , find

$$\Theta^s = \arg \min_{\Theta \in \mathcal{S}} \sum_{i=1}^n \int_{\Omega} u_i^s F_i(\Theta_1, \dots, \Theta_n) dx.$$

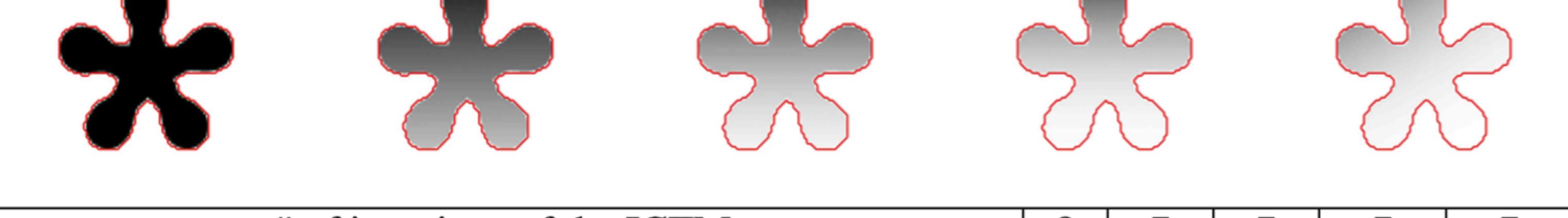
2. For $i \in [n]$, evaluate

$$\phi_i^s = F_i(\Theta_1^s, \dots, \Theta_n^s) + \lambda \sum_{j=1, j \neq i}^n \sqrt{\frac{\pi}{\tau}} G_{\tau} * u_j^s.$$

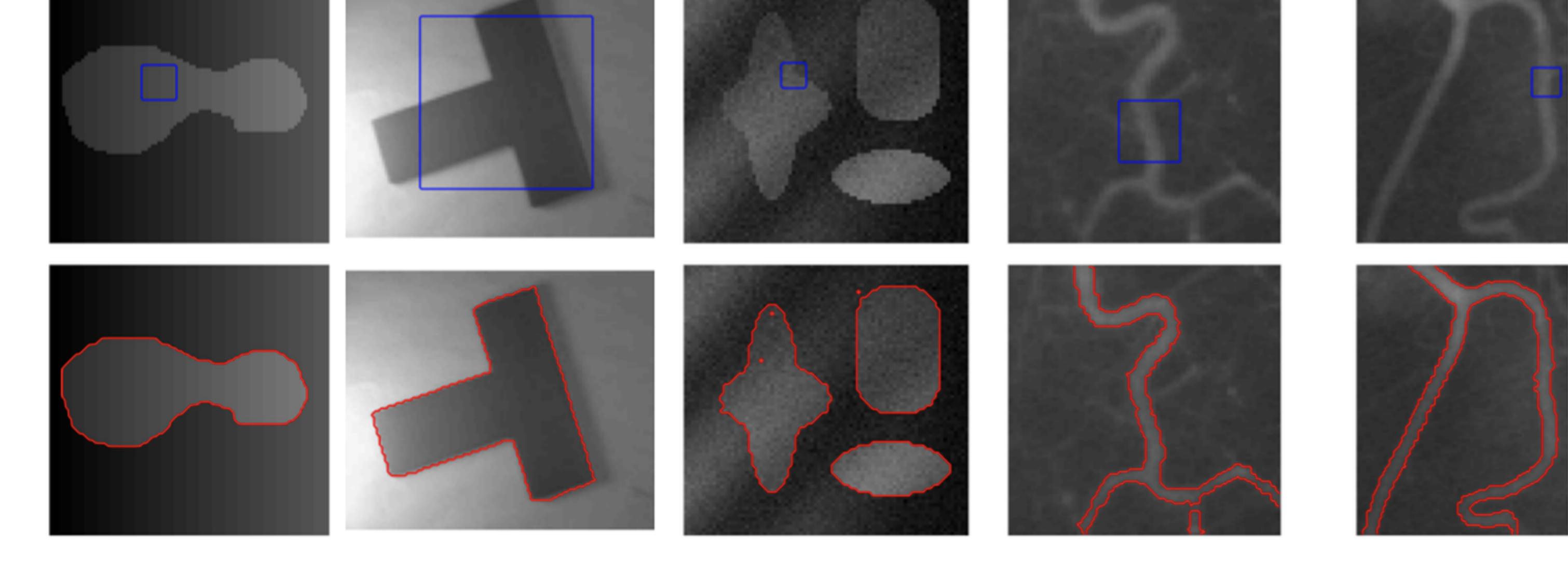
3. For $i \in [n]$, set

$$u_i^{s+1}(x) = \begin{cases} 1 & \text{if } i = \min\{\arg \min_{\ell \in [n]} \phi_{\ell}^s\}, \\ 0 & \text{otherwise.} \end{cases}$$

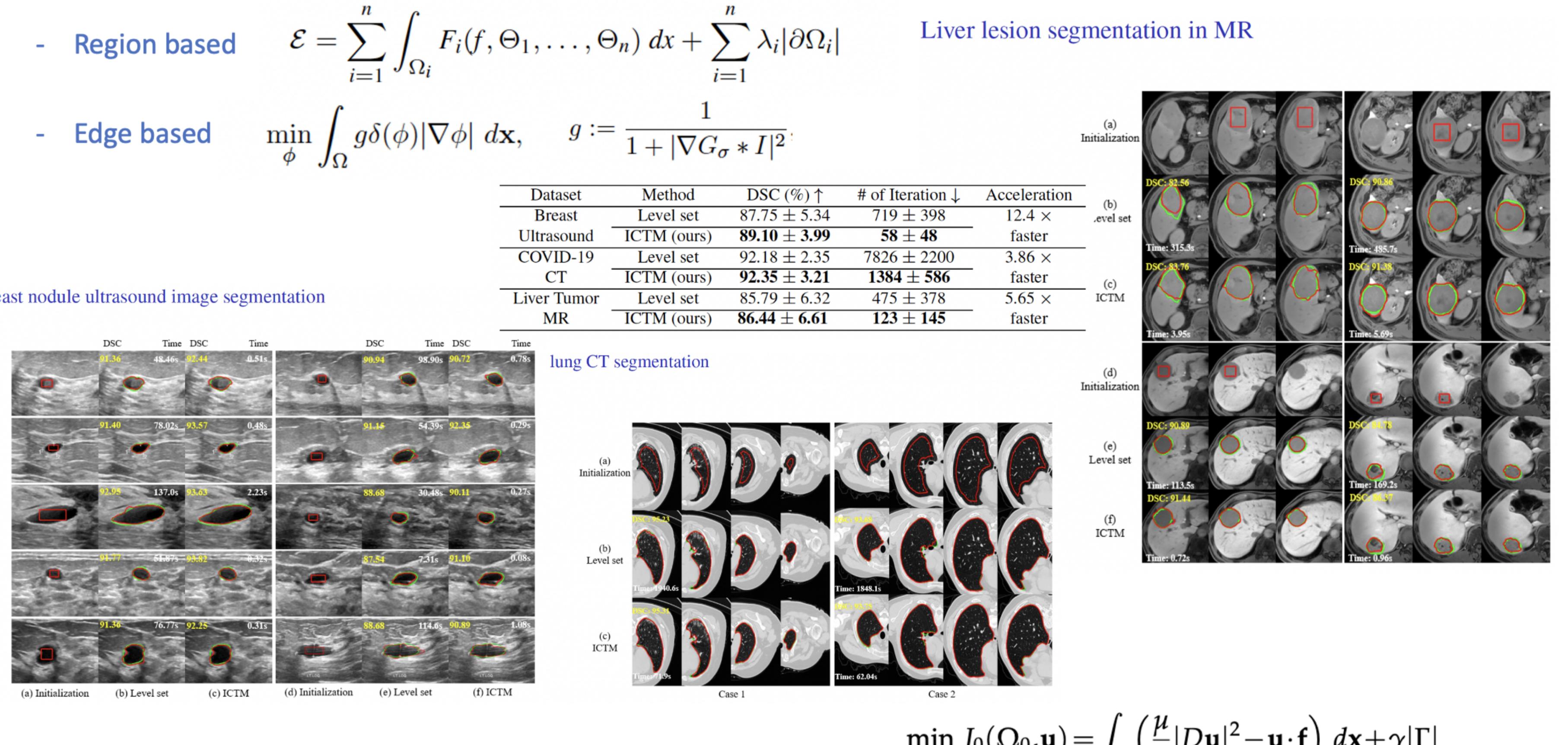
Numerical Results



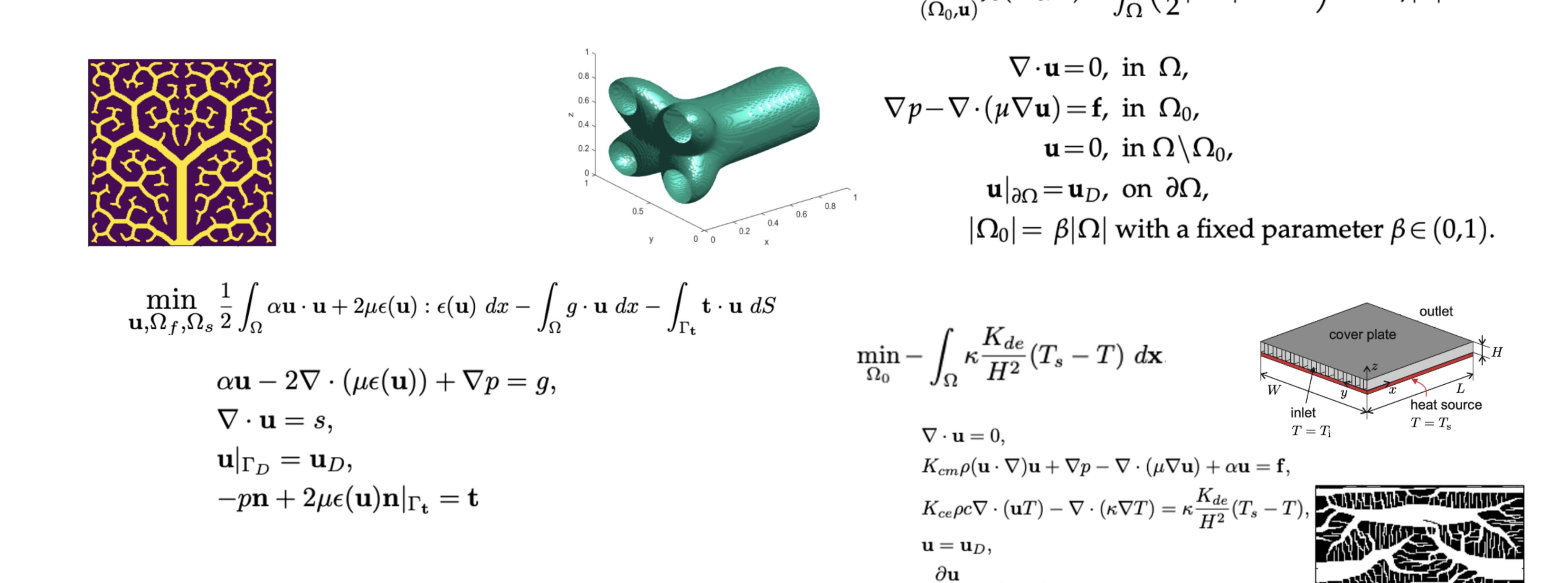
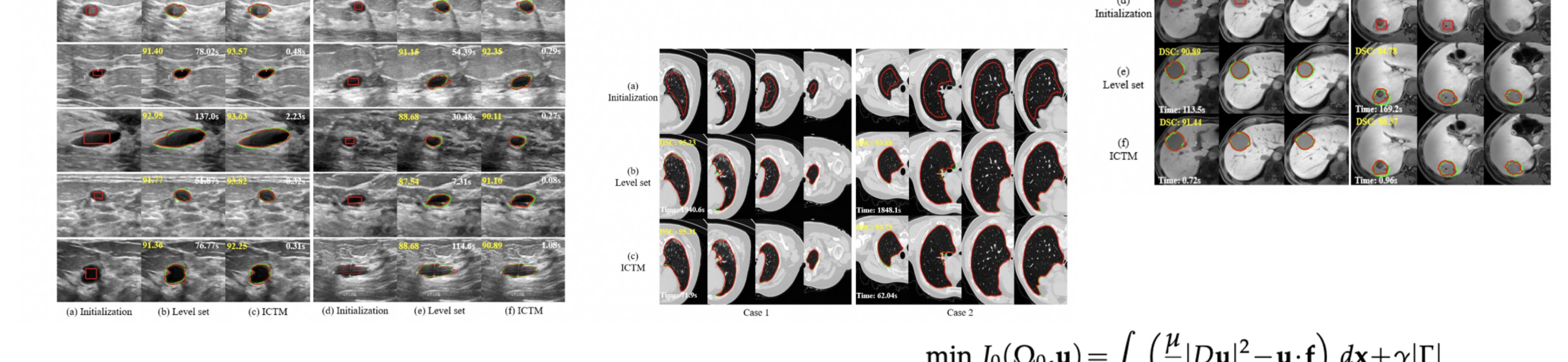
# of iterations of the ICTM	8	7	7	7	7
# of iterations of the level-set method [Zhang et al., 2016]	7	13	35	186	239



# of iterations of the ICTM	13	25	43	28	47
# of iterations of the level-set method [Li et al., 2008]	29	256	131	117	209



Liver nodule ultrasound image segmentation



$$\min_{(\Omega_0, \mathbf{u})} J_0(\Omega_0, \mathbf{u}) = \int_{\Omega} \left(\frac{\mu}{2} |\mathbf{D}\mathbf{u}|^2 - \mathbf{u} \cdot \mathbf{f} \right) dx + \gamma |\Gamma|$$

$$\nabla \cdot \mathbf{u} = 0, \text{ in } \Omega, \quad \nabla p - \nabla \cdot (\mu \mathbf{D}\mathbf{u}) = \mathbf{f}, \text{ in } \Omega_0, \quad \mathbf{u} = 0, \text{ in } \Omega \setminus \Omega_0, \quad \mathbf{u}|_{\partial \Omega} = \mathbf{u}_D, \text{ on } \partial \Omega, \quad |\Omega_0| = \beta |\Omega| \text{ with a fixed parameter } \beta \in (0, 1).$$

$$\min_{\Omega_0} \int_{\Omega_0} \alpha \mathbf{u} : \mathbf{e}(\mathbf{u}) dx + 2\mu \epsilon(\mathbf{u}) : \mathbf{e}(\mathbf{u}) dx - \int_{\Omega} g \cdot \mathbf{u} dx - \int_{\Gamma_1} \mathbf{t} \cdot \mathbf{u} ds - \alpha \mathbf{u} - 2\mathbf{v} \cdot (\mu \mathbf{e}(\mathbf{u})) + \nabla p = g, \quad \nabla \cdot \mathbf{u} = s, \quad \mathbf{u}|_{\Gamma_D} = \mathbf{u}_D, \quad -pn + 2\mu \epsilon(\mathbf{u}) \mathbf{n}|_{\Gamma_1} = \mathbf{t}$$

$$\min_{\Omega_0} - \int_{\Omega_0} \frac{K_{de}}{H^2} (T_s - T) dx \quad \nabla \cdot \mathbf{u} = 0, \quad K_{ce} \rho (\mathbf{u} \cdot \nabla) \mathbf{u} + \nabla p - \nabla \cdot (\kappa \nabla \mathbf{u}) + \alpha \mathbf{u} = \mathbf{f}, \quad K_{ce} \rho c (\mathbf{u} \cdot \nabla) \mathbf{u} - \nabla \cdot (\kappa \nabla \mathbf{u}) = \kappa \frac{K_{de}}{H^2} (T_s - T), \quad \mathbf{u}|_{\partial \Omega} = \mathbf{u}_D, \quad \frac{\partial \mathbf{u}}{\partial \mathbf{n}} - pn = \mathbf{g}, \quad T = t_D, \quad \frac{\partial T}{\partial \mathbf{n}} = 0,$$

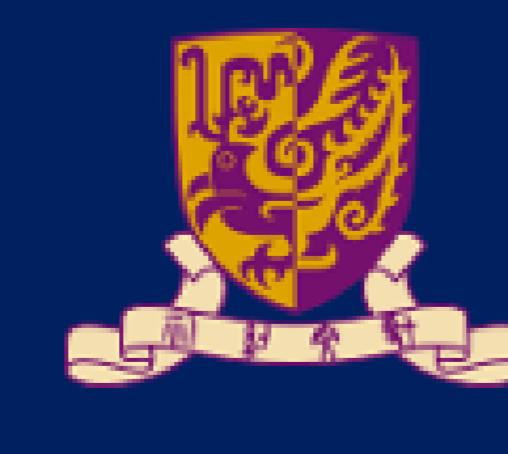


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